

Modelling of a Single Cardiomyocyte
Interaction with a Microcantilever Using COMSOL
Multiphysics

By Indradumna Banerjee
Department of Automation Science and
Engineering,
Tampere University Of Technology

Introduction

- Cardiac muscle consists of interlacing bundles of cardiomyocytes (muscle cells)
Cardiomyocytes are narrower and much shorter than skeletal muscle cells, being about 0.02 mm wide and 0.1 mm long.
- With the discovery of iPS cells, currently efforts are underway to generate cardiomyocytes in vitro.
- Use of iPS cell derived cardiomyocytes will require careful characterization of their properties.
- If it is possible to measure contractile properties of a single cardiomyocyte cell, then it can lay the foundation for quantitatively understanding the mechanism of heart failure and molecular alterations in diseased heart cells.

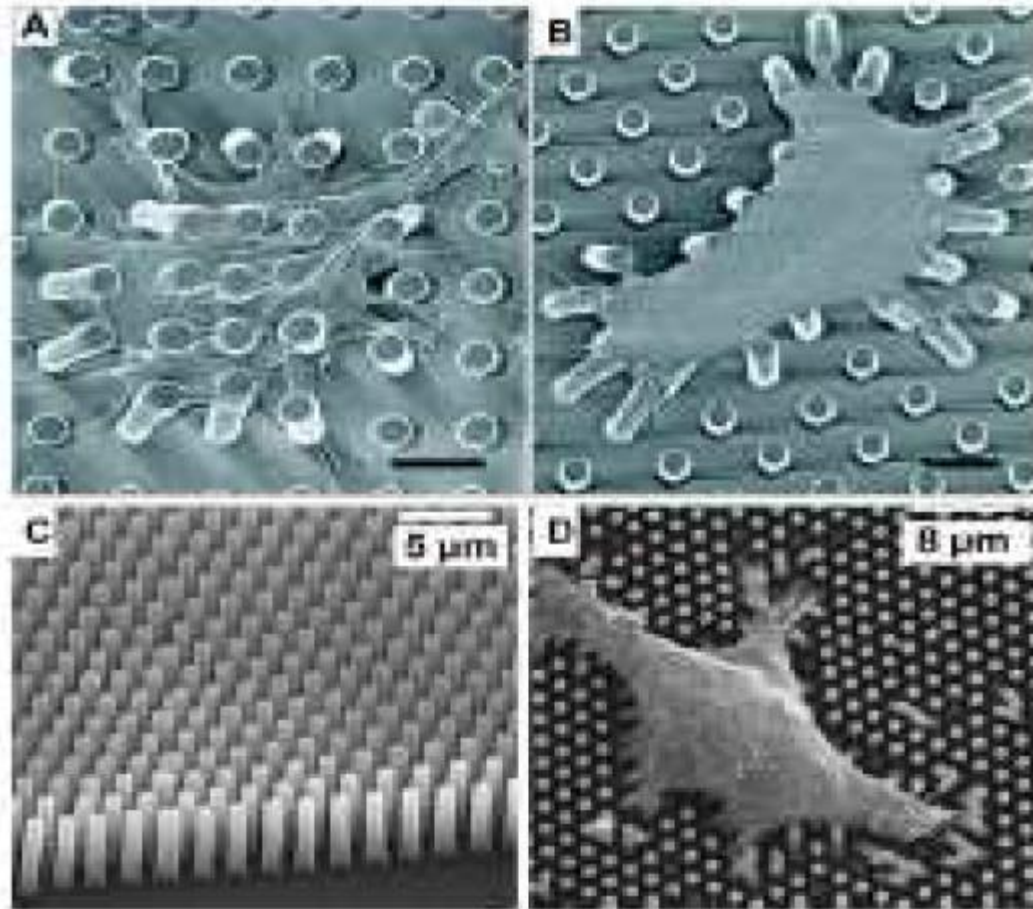
Background and governing equations

- Navier stoke's equation for describing the flow of incompressible fluids where \mathbf{u} is the velocity field p is the pressure .

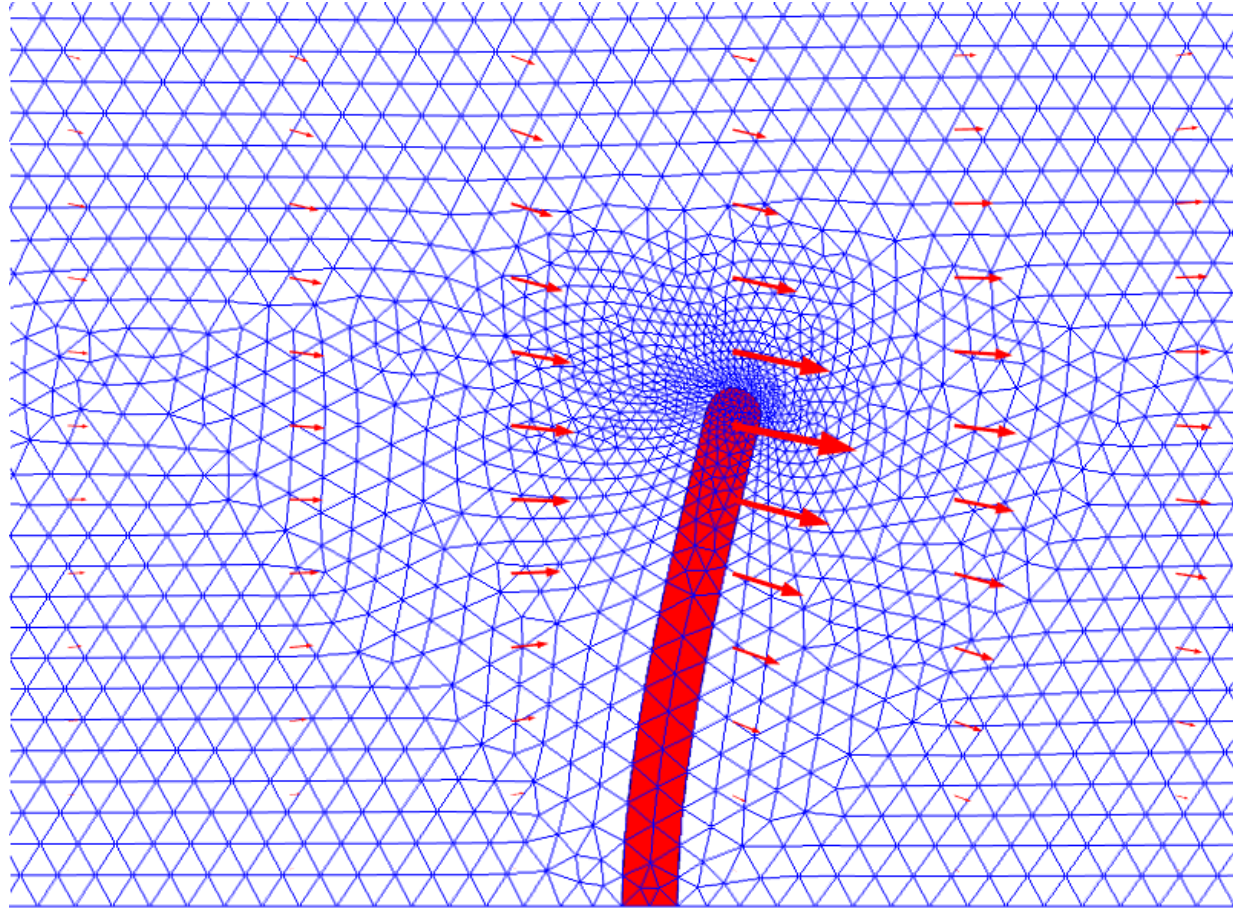
$$\rho \frac{\partial \mathbf{u}}{\partial t} - \nabla \cdot [-p \mathbf{I} + \eta (\nabla \mathbf{u} + (\nabla \mathbf{u})^T)] + \rho ((\mathbf{u} - \mathbf{u}_m) \cdot \nabla) \mathbf{u} = \mathbf{F}$$
$$-\nabla \cdot \mathbf{u} = 0$$

- Cellular substrate is considered as an incompressible fluid over a bed of vertical microcantilevers.

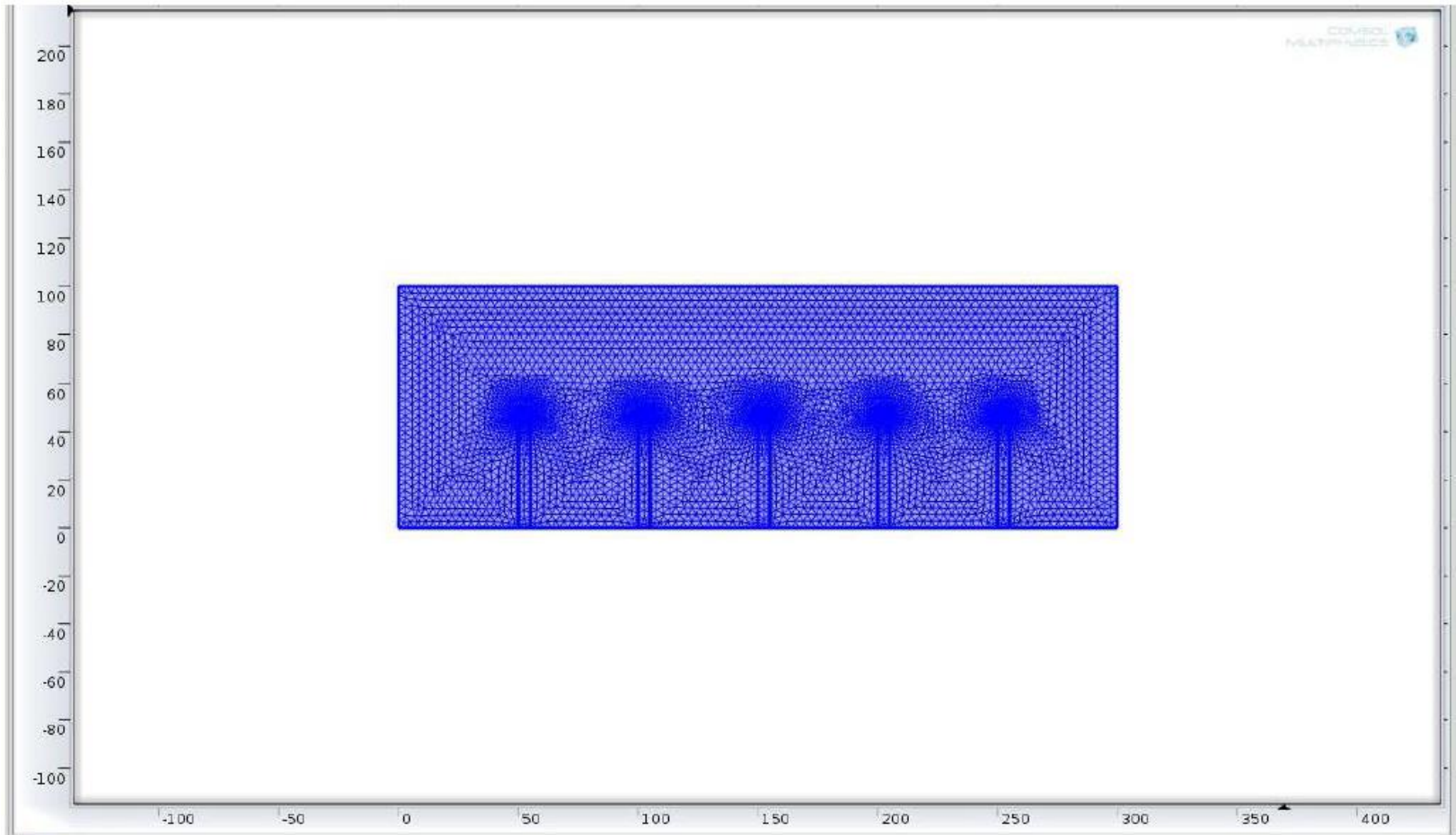
Array of Vertical Microcantilevers



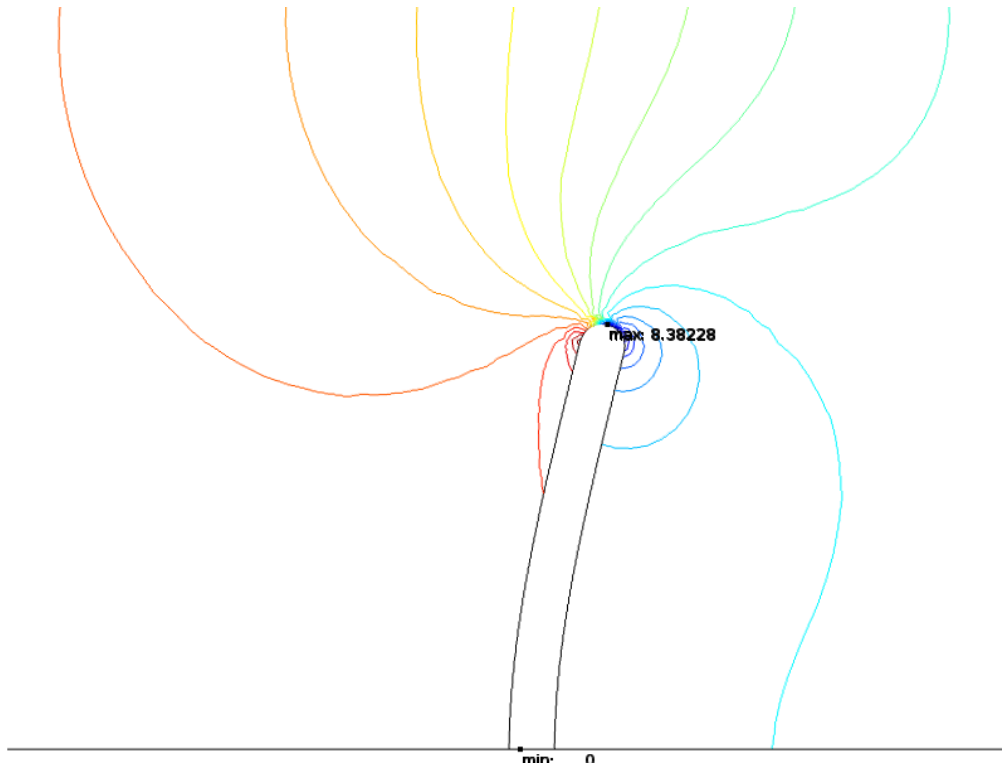
Simulations – Single cantilever deflection



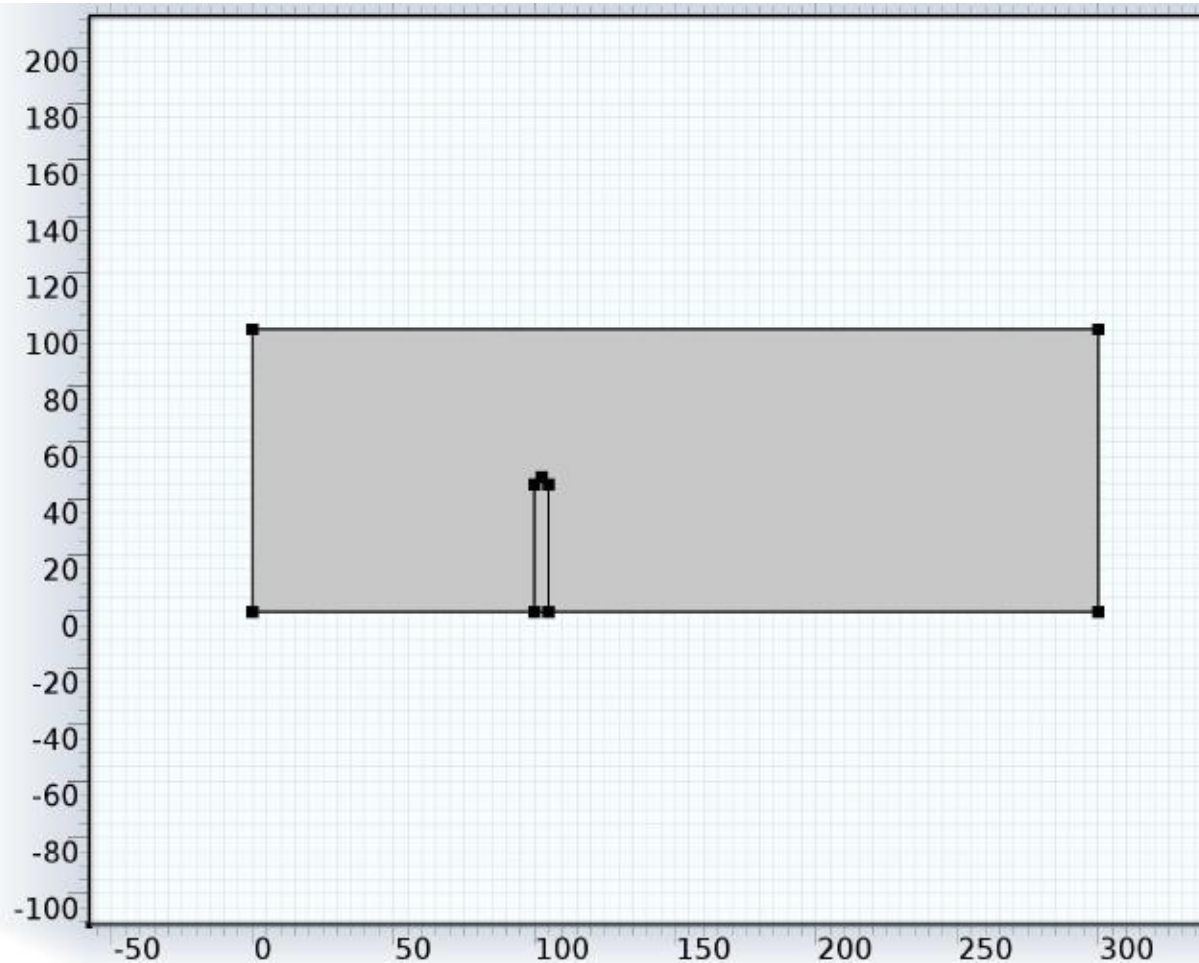
Simulations – multiple cantilever deflection



Simulation – Pressure and Displacement



Geometry should look like:



Simulation conditions

- Density – 950 kg/m^3
- Viscosity – $0.78 \times 10^{-3} \text{ kg/m}^3$
- Stiffness constant – 0.002 N/m
- Maximum Deflection produced : $8.3 \text{ } \mu\text{m}$.
- Microcantilever dimensions – $500 \text{ } \mu\text{m}$ in length, $100 \text{ } \mu\text{m}$ in width, $0.9 \text{ } \mu\text{m}$ in thickness
- Estimated forces in the range of nanonewtons in sync with actual measured values.

References

- [1] Mijailovich, S., Kojic, M., Zivkovic, M., Fabry, B., Fredberg, J. A finite element model of cell deformation during magnetic bead twisting. *Journal of Applied Physiology* 93, 1429–1436, 2002.
- [2] Satcher, R., Dewey, C. Theoretical estimates of mechanical properties of the endothelial cell cytoskeleton. *Biophys. J.* 71, 109–118, 1996.
- [3] Deshpande, V. S., McMeeking, R. M., Evans, A. G. A bio-chemo-mechanical model for cell contractility. *PNAS* 103, 14015–14020, 2006.
- [4] Ingber DE, Tensegrity I. Cell structure and hierarchical systems biology. *J. Cell Sci.* 116, 1157-1173, 2003.
- [5] Ingber DE Tensegrity II. How structural networks influence cellular information processing networks. *J. Cell Sci.* 116, 1397-1408, 2003.
- [6] Addae-Mensah K, Wikswo J (2008) Measurement techniques for cellular biomechanics in vitro. *Exp Biol Med* 233(7):792–809.